



Acceleration of DNA repair by charge-transport: stochastic analysis and deterministic models

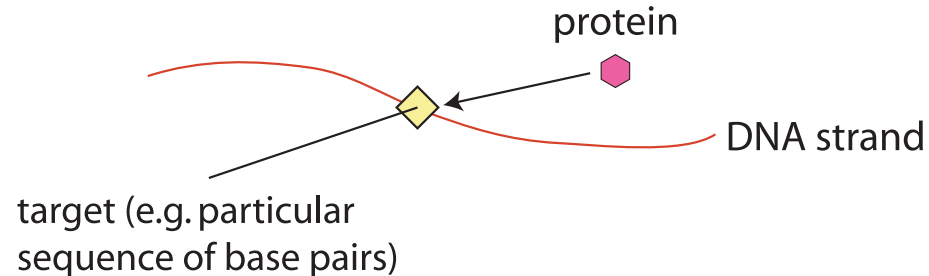
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Background and Motivation

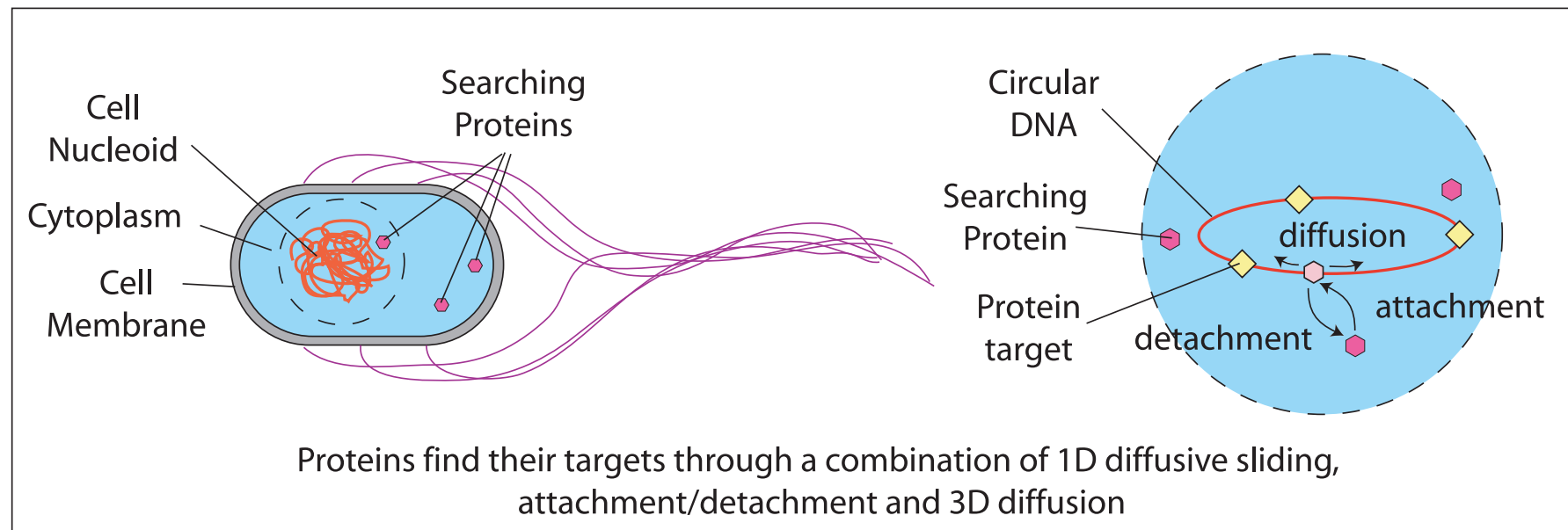
- DNA-protein interactions are important in gene transcription and protein production



- But: rates of DNA-protein reactions are faster than the theoretical upper limit predicted by 3D diffusive (Debye-Smoluchowski) theory. [Riggs *et al.* 1970]
- And: rates of reactions also faster than typical 1D diffusive sliding time. For *E. coli*, $L \sim 10^6$ bp $D \sim 5 \times 10^6$ bp²/s $\Rightarrow T \sim L^2/D \approx 2$ days
- Question: how do proteins/enzymes find their targets on DNA so quickly? [Berg *et al.* 1981, Von-Hippel and Berg, 1987]

Proposed solution

- Facilitated diffusion [Berg 1981]: combination of 1D sliding and 3D diffusion \Rightarrow rates predicted to increase up to $100\times$.



- However, acceleration requires D_{1D} and D_{3D} to be comparable and equal time spent in 1D and 3D diffusion.
- This is not true in most situations!



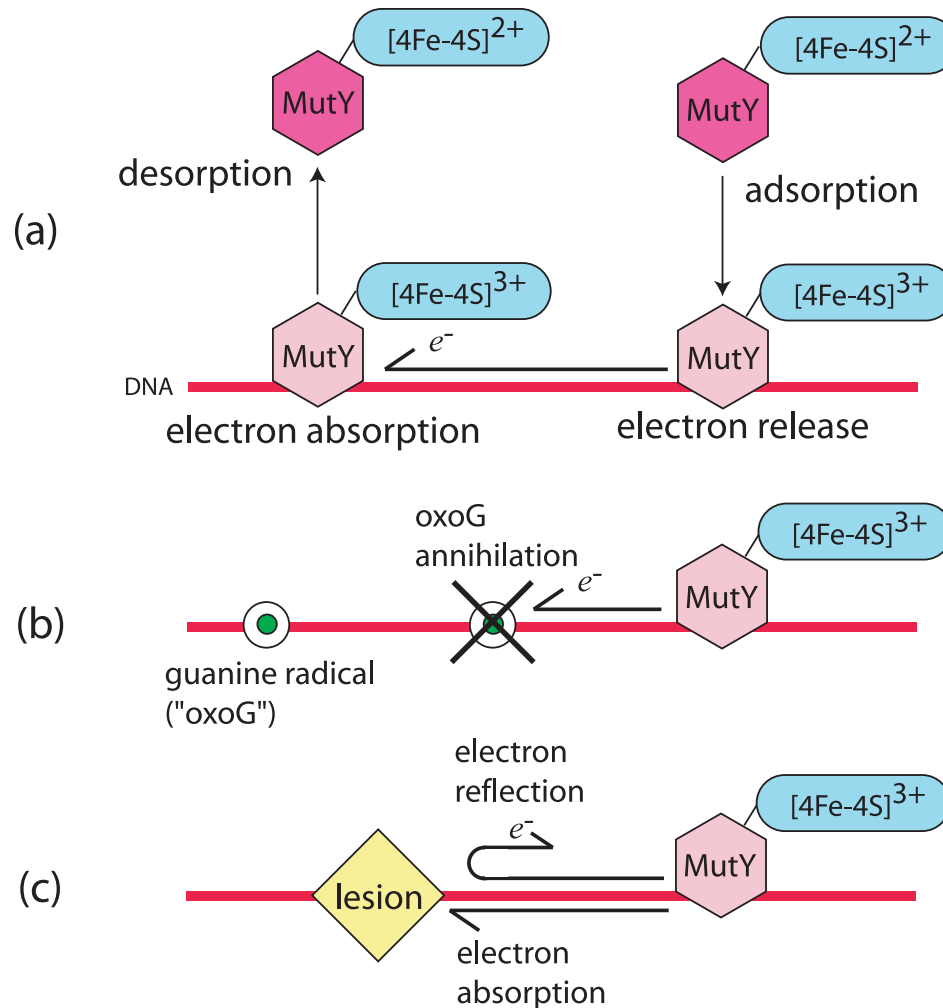
Other mechanisms

- Fast intersegmental transfers [Sheinman and Kafri 2008]
- Effect of DNA conformation [Hu *et al.* 2006]
- Protein cooperativity [Cherstvy *et al.* 2008]
- Charge Transport [Yavin *et al.* 2005, Boon *et al.* 2003]: applicable to a particular protein called MutY, a Base Excision Repair enzyme.

Base Excision Repair (BER) enzymes

- The genome of all living organisms is constantly under attack by mutagenic agents e.g. ionizing radiation
- Mutagenic agents give rise to damaged base pairs in DNA (“lesions”) \Rightarrow miscoded proteins, possibly cancer.
- BER enzymes locate lesions on DNA, remove them, maintain integrity of genome.
- MutY searches for lesions via a Charge-Transport (CT) mechanism [Yavin *et al.* 2005, Boon *et al.* 2003]

Charge Transport (CT)

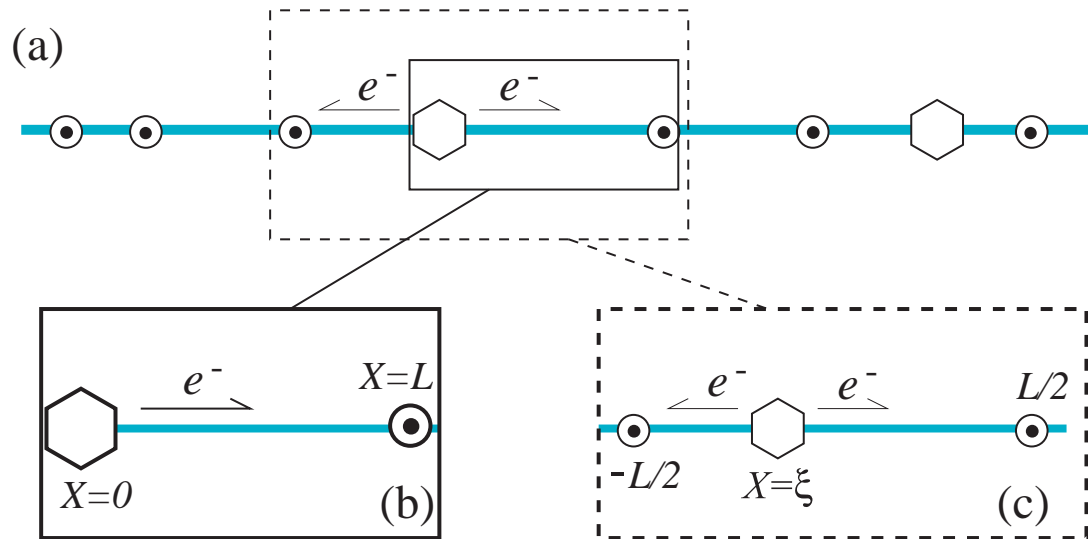


(a) Iron-Sulfur cofactors oxidize when MutY adsorbs to DNA. Release/absorption of electrons \Leftrightarrow adsorption/desorption of enzyme.

(b) Guanine radicals ("OxoGs"): damaged bases that annihilate upon absorbing an electron.

(c) Lesions prevent passage of electrons by reflection/absorption. They require presence of MutY to be excised from DNA.

Stochastic Broadwell Model



Note: electron return probability = 1 in absence of guanine radicals

One-sided Broadwell problem

- Governing equations [Bicout, 1997, Fok *et al.* 2008]:

$$\begin{aligned}\frac{\partial P_+}{\partial T} + V \frac{\partial P_+}{\partial X} &= -FP_+ + FP_- - MP_+ \\ \frac{\partial P_-}{\partial T} - V \frac{\partial P_-}{\partial X} &= FP_+ - FP_- - MP_-\end{aligned}$$

$P_{\pm}(X, T)$: pdfs of rightward and leftward electron, V : electron speed, F : flip rate, M : decay rate

- Boundary conditions:

$$P_+(0, T) = P_-(L, T) = 0$$

- Initial conditions:

$$\begin{aligned}P_+(X, 0) &= \delta(X) \\ P_-(X, 0) &= 0\end{aligned}$$

Dimensionless eqns

Non-dimensionalize space by $1/\rho$, time by $1/\rho V$ where $\rho = \text{OxoG density}$:

$$x = \rho X, \quad t = \rho V T,$$

$$\Rightarrow \frac{\partial \mathbf{Q}}{\partial t} = \mathbf{L} \mathbf{Q}, \quad \mathbf{Q} = \begin{pmatrix} Q_+(x, t) \\ Q_-(x, t) \end{pmatrix},$$

where $Q_{\pm} = P_{\pm}/\rho$ and

$$\mathbf{L} = \begin{bmatrix} -\frac{\partial}{\partial x} - f - \mu & f \\ f & \frac{\partial}{\partial x} - f - \mu \end{bmatrix},$$

and

$$f = \frac{F}{\rho V}, \quad \mu = \frac{M}{\rho V}.$$

Adsorption/desorption probabilities

Take $\mu = 0$ always (no electron decay)

$$\text{Desorption prob: } \int_0^\infty Q_-(0, t') dt' = \frac{f\ell}{1 + f\ell}$$

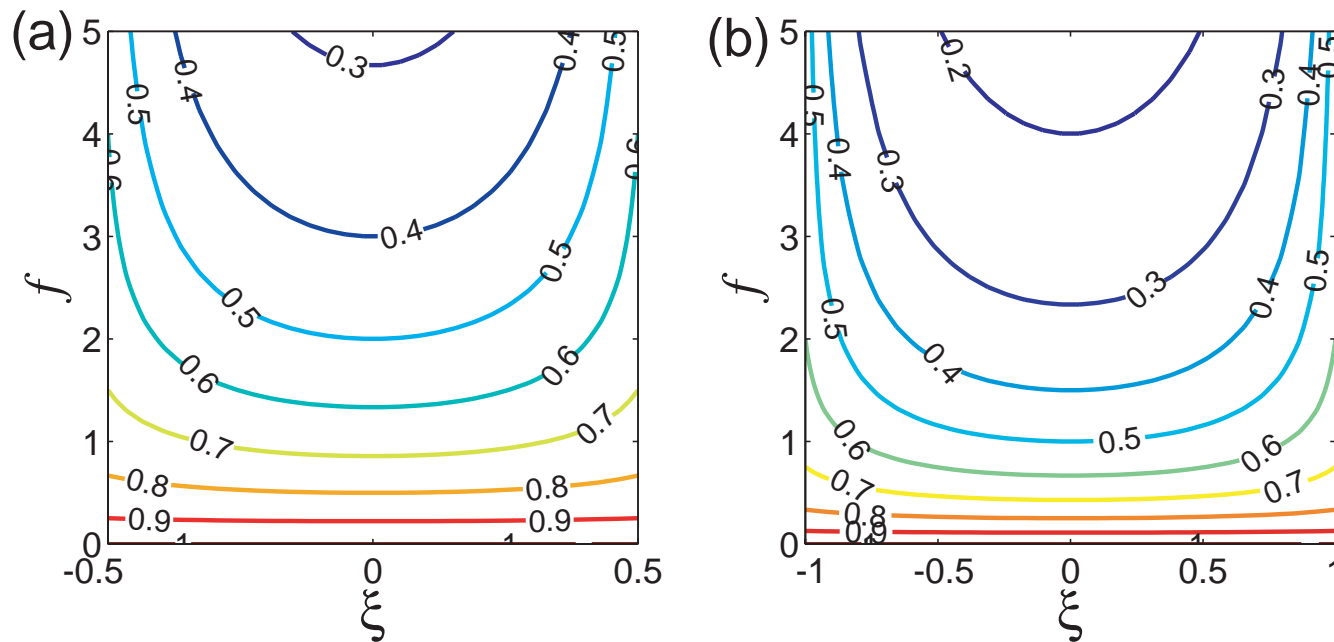
$$\text{Adsorption prob: } \int_0^\infty Q_+(L, t') dt' = \frac{1}{1 + f\ell}$$

Extension to two-sided problem:

$$\Pi_{\text{desorb}} = \frac{1}{2} \left[\frac{f(\ell/2 - \xi)}{1 + f(\ell/2 - \xi)} + \frac{f(\ell/2 + \xi)}{1 + f(\ell/2 + \xi)} \right]$$

$$\Pi_{\text{adsorb}} = \frac{1}{2} \left[\frac{1}{1 + f(\ell/2 - \xi)} + \frac{1}{1 + f(\ell/2 + \xi)} \right]$$

Sticking probability



Dependence of enzyme sticking probability Π_{adsorb} on its landing position ξ and flipping rate for gap size (a) $\ell = 1$ and (b) $\ell = 2$.

$f \ll 1$: ballistic limit, $f \gg 1$: diffusive limit

Adsorption Statistics away from lesions

1. Average over landing position ξ :

$$\begin{aligned}\bar{\Pi}_{\text{adsorb}} &= \frac{1}{2\ell} \int_{-\ell/2}^{\ell/2} \Pi_{\text{adsorb}}(\xi, \ell; f) d\xi \\ &= \frac{2}{f\ell} \tanh^{-1} \left(\frac{f\ell}{2 + f\ell} \right).\end{aligned}$$

2. Consider gaps with discrete distribution $\ell_1, \ell_2, \ell_3, \dots$. Assume a fraction ϕ_j of gaps have size ℓ_j . Deposit a single enzyme onto the DNA. The probability of landing in gap of size ℓ_j is $\phi_j \ell_j / \sum_{j=1}^{\infty} \phi_j \ell_j$. Fraction that *stays adsorbed* in gap of size ℓ_j is

$$\frac{2}{f\ell_j} \tanh^{-1} \left(\frac{f\ell_j}{2 + f\ell_j} \right) \times \frac{\phi_j \ell_j}{\sum_{j=1}^{\infty} \phi_j \ell_j}$$

Continuous gap size distribution: $\ell_j \rightarrow \ell, \phi_j \rightarrow \phi(\ell)d\ell$:

$$\text{Ensemble average } \langle \bar{\Pi}_{\text{adsorb}} \rangle = \frac{2}{f\langle \ell \rangle} \int_0^{\infty} \phi(\ell) \tanh^{-1} \left(\frac{f\ell}{2 + f\ell} \right) d\ell.$$

Form of $\phi(\ell)$?

If OxoGs randomly appear anywhere on an infinite DNA, what is the pdf of the gap size (distance between 2 consecutive OxoGs)?

Consider a lattice of length L_0 with n sites (each site has width a) where OxoGs can appear with rate Ω radicals per unit time T per lattice site. Time taken for G radicals to appear is $T_0 = G/n\Omega$.

Let $N(m, T)$ be the pdf of the number of gaps of size m . Then N obeys [D'Orsogna and Chou 2005]

$$\frac{1}{\Omega} \frac{\partial N(m, T)}{\partial T} = 2 \sum_{m'=m+1}^n N(m', T) - mN(m, T)$$

Define $\rho \equiv G/L_0$ as the OxoG density and the dimensionless variables

$$y = \rho am, \quad t = T/T_0, \quad p = N/Gt = \text{gap fraction}$$

Take continuum limit $n \rightarrow \infty$, $a\rho \rightarrow 0$ and $G, L_0 \rightarrow \infty$ such that ρ remains fixed.

$$p(y, t) \rightarrow \text{probability density for continuous gap size } y$$

Gap distribution

Setting $q(y, t) = tp(y, t)$ where $p(y, t)$ is the continuous pdf of gaps of size y :

$$\frac{\partial q}{\partial t} = 2 \int_y^\infty q(y', t) dy' - yq(y, t)$$

Solve by Laplace transform in time:

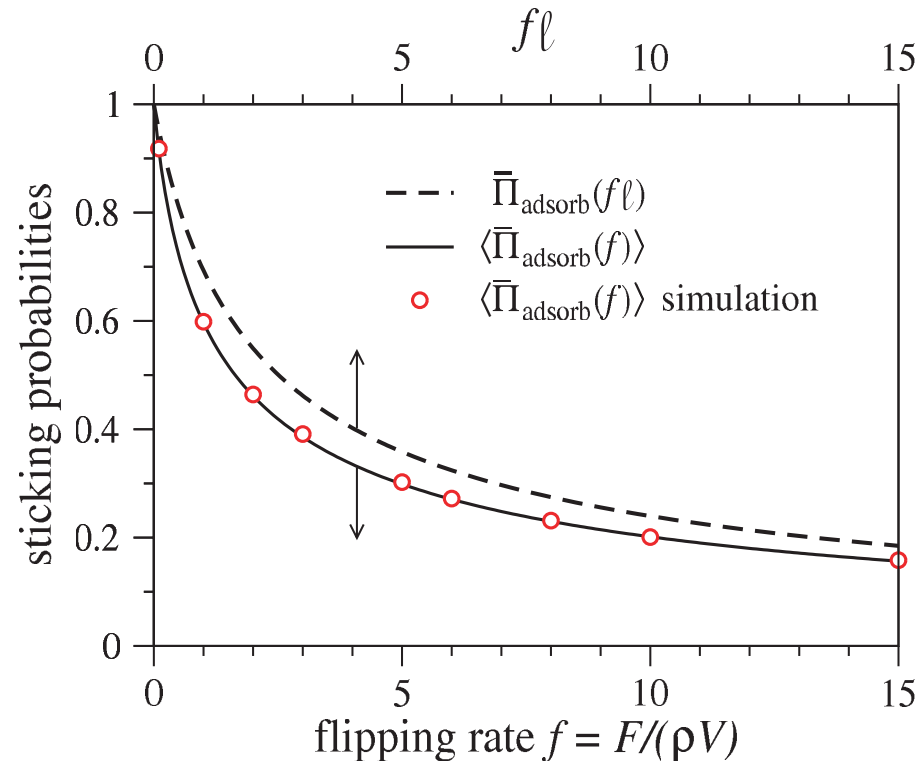
$$\begin{aligned}\Rightarrow q(y, t) &= t^2 e^{-yt} \\ \Rightarrow p(y, t = 1) &= e^{-y} \\ \Rightarrow \text{Prob}(y \leq Y \leq y + dy) &= e^{-y} dy \equiv \phi(y) dy\end{aligned}$$

Y : non-dimensional gap length at $t = 1 \Leftrightarrow G$ radicals have appeared. Hence,

$$\langle \bar{\Pi}_{\text{adsorb}} \rangle = \frac{e^{1/f} \text{Ei}(1/f)}{f}$$

where $\text{Ei}(x) = \int_x^\infty \frac{e^{-t}}{t} dt$

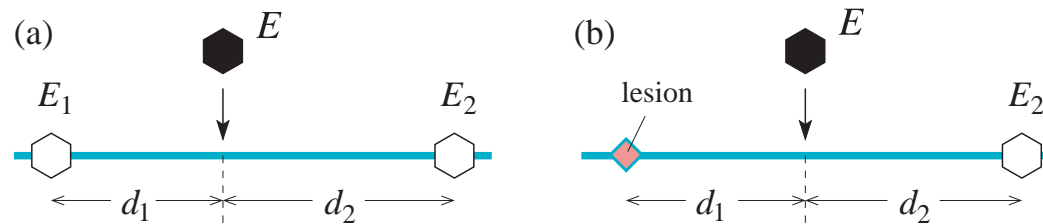
Verification



Sticking probabilities for deposition of a single enzyme onto an infinite DNA with gap distribution $\phi(\ell) = e^{-\ell}$. Also expect probabilities to be approximately valid when the fraction of OxoGs annihilated is $\ll 1$.

Colocalization of enzymes near lesions

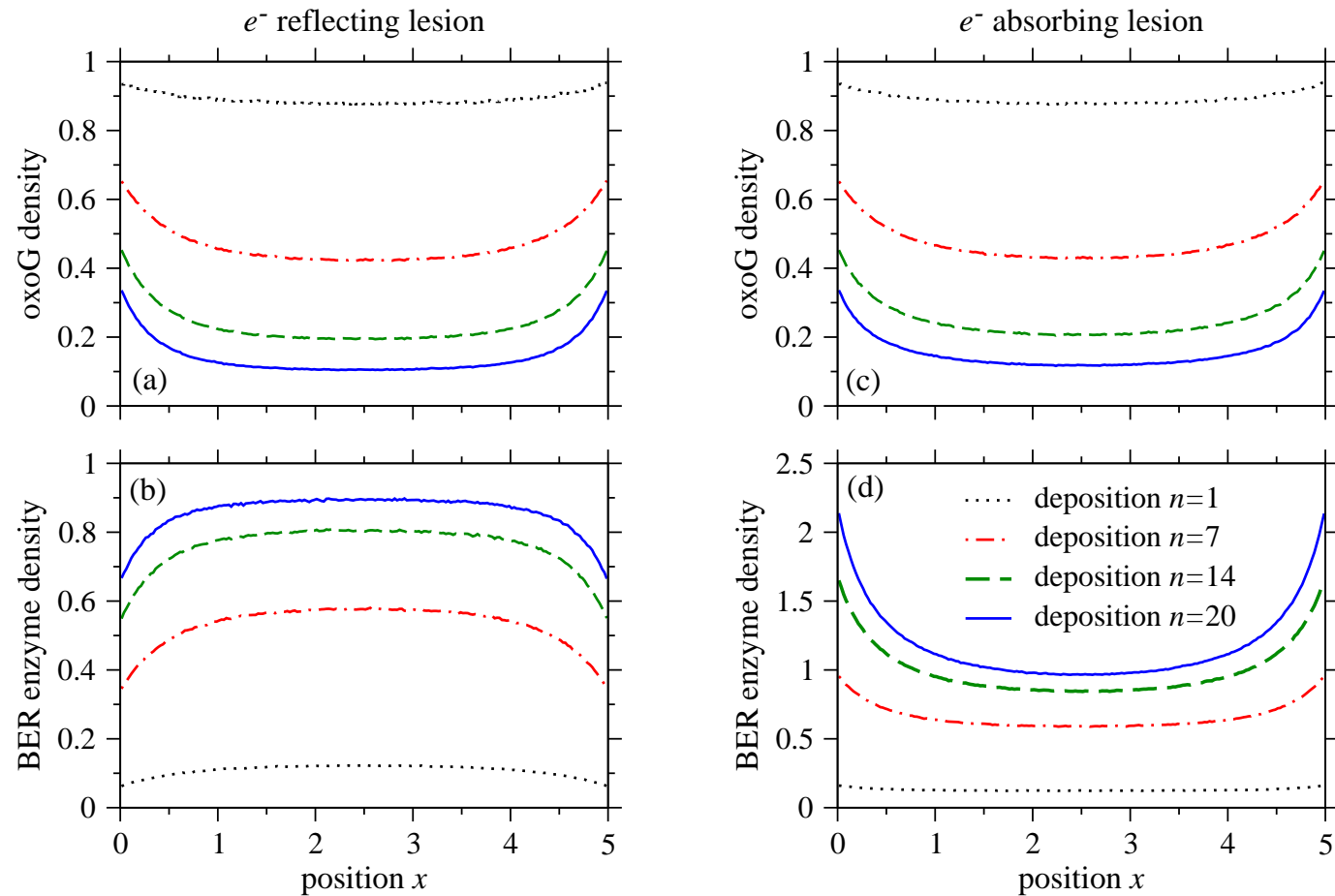
Analyze using Monte Carlo with adsorption/desorption probabilities Π_{adsorb} and Π_{desorb} :



(a)	Event:	E self-desorbs	E adsorbs, E_1 desorbs	E adsorbs, E_2 desorbs
	Probability:	$\frac{1}{2} \left(\frac{f d_1}{1+f d_1} + \frac{f d_2}{1+f d_2} \right)$	$\frac{1}{2} \frac{1}{1+f d_1}$	$\frac{1}{2} \frac{1}{1+f d_2}$

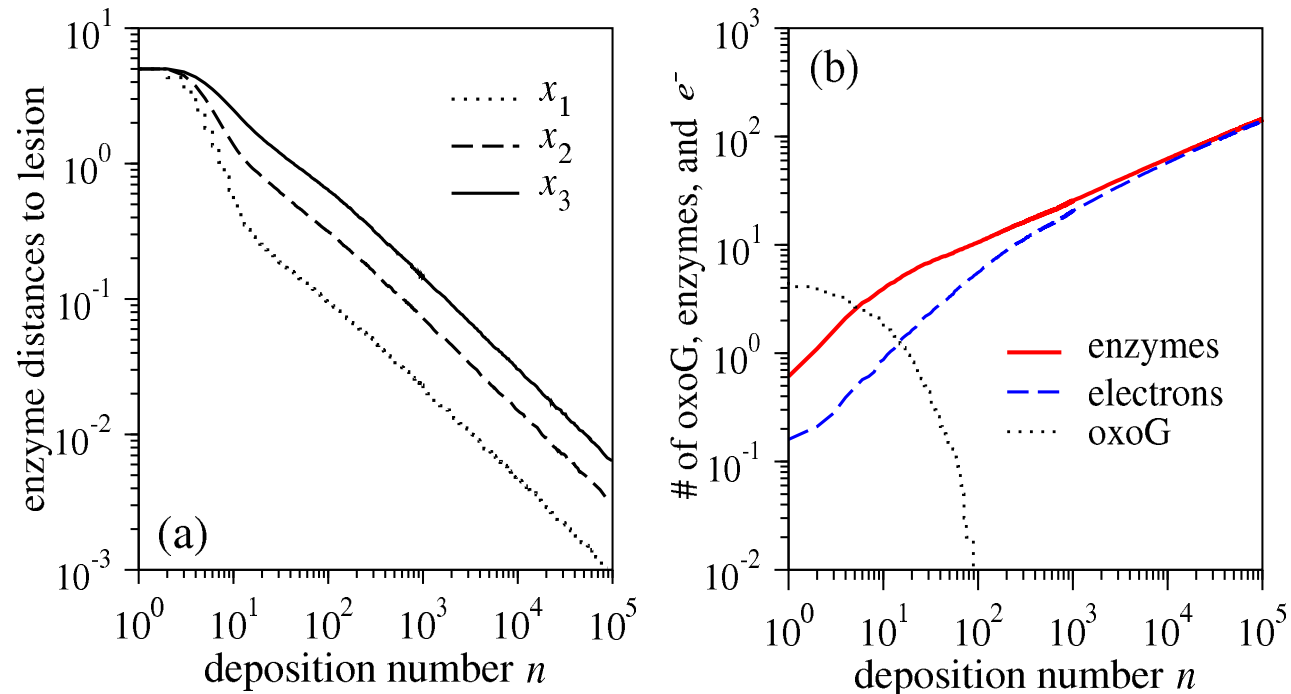
(b)	Event:	E self-desorbs	E adsorbs, E_2 stays adsorbed	E adsorbs, E_2 desorbs
	Prob: (reflecting lesion)	$\frac{1}{2} + \frac{1}{2} \left(\frac{f d_2}{1+f d_2} \right)$	0	$\frac{1}{2} \frac{1}{1+f d_2}$
	Prob: (absorbing lesion)	$\frac{1}{2} \left(\frac{f d_1}{1+f d_1} + \frac{f d_2}{1+f d_2} \right)$	$\frac{1}{2} \frac{1}{1+f d_1}$	$\frac{1}{2} \frac{1}{1+f d_2}$

MC Results (1/2)



Evolution of enzyme density as enzymes are *adiabatically* deposited onto DNA. Results came from averaging 10^7 trials using flip rate $f = 1$.

MC Results (2/2)



Scaling results in large n limit. (a) x_i = distance from lesion to i th closest enzyme. Convergence of repair enzymes = $O(n^{-2/3})$. (b) Accumulation of enzymes = $O(n^{1/3})$.

Enzyme deposition within 5 base pairs of a lesion requires $n \approx 6 \times 10^6$ deposition attempts. If each deposition takes 0.0005s \Rightarrow total search time \approx 50 minutes.

Discussion

- Compare with randomly deposited “passive” enzymes that always stick to the DNA. $n \gg 1$: number of depositions

	Passive	CT
Enzyme number :	$O(n)$	$O(n^{1/3})$
enzyme-lesion distance :	$O(n^{-1})$	$O(n^{-2/3})$

- Passive enzymes converge more quickly but search is very redundant/wasteful.
- CT search strategy more effective when number of enzymes in system is limited.

Weaknesses of model

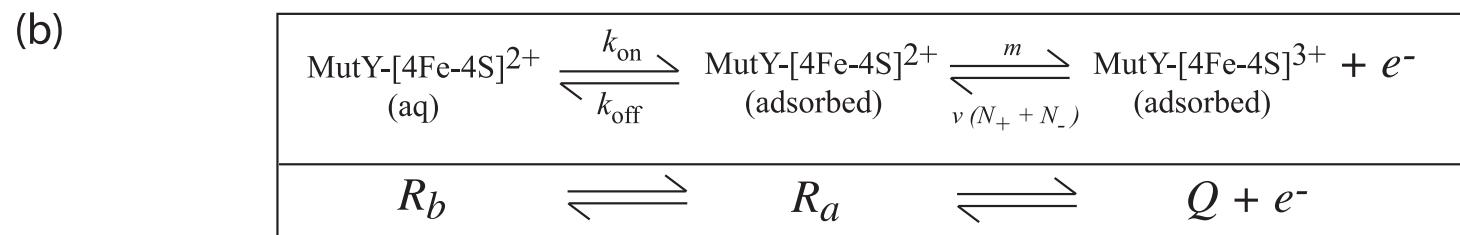
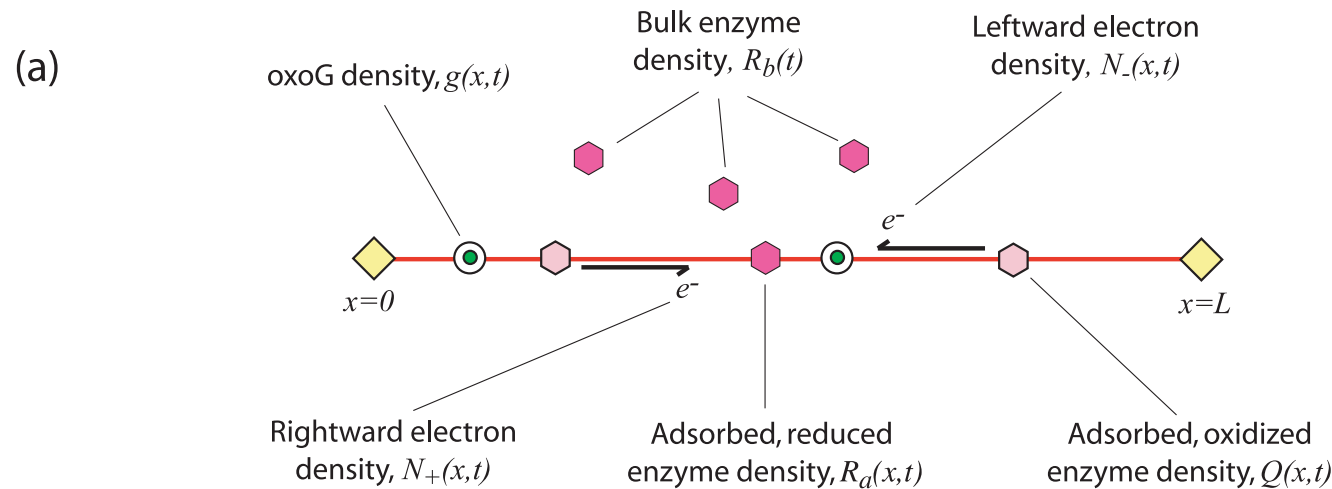
- Search time of 50 minutes is an improvement, but it is still too slow.
- Enzymes are stationary on DNA; they do not diffuse along strand.
- MC simulations keep bulk chemical potential constant. Number of enzymes on DNA can grow without bound.
- Assumed adiabatic depositions.

All these factors make the discrete model rather unrealistic.

Improvements:

- Use a continuum PDE model
- Model enzyme binding more carefully

Binding kinetics



Discrete model assumed electron release prob = 1 upon contact with DNA, desorption prob = 1 upon electron absorption. This is **not** the same as taking $m, k_{\text{off}} \rightarrow \infty$.

PDE model for CT enzymes

$$\frac{\partial Q}{\partial t} = D_+ \frac{\partial^2 Q}{\partial x^2} - v(N_+ + N_-)Q + mR_a,$$

$$\frac{\partial R_a}{\partial t} = D_- \frac{\partial^2 R_a}{\partial x^2} + v(N_+ + N_-)Q - k_{\text{off}}R_a + k_{\text{on}} \left(\frac{\Omega}{L} \right) R_b - mR_a,$$

$$\frac{dR_b}{dt} = -k_{\text{on}}R_b + \frac{k_{\text{off}}}{\Omega} \int_0^L R_a dx,$$

$$\frac{\partial N_+}{\partial t} + v \frac{\partial N_+}{\partial x} = fN_- - fN_+ - vN_+(Q + g) + \frac{mR_a}{2},$$

$$\frac{\partial N_-}{\partial t} - v \frac{\partial N_-}{\partial x} = -fN_- + fN_+ - vN_-(Q + g) + \frac{mR_a}{2},$$

$$\frac{\partial g}{\partial t} = -v(N_+ + N_-)g.$$

Q : Oxidized enzyme on DNA, R_a : reduced enzyme on DNA, R_b : reduced enzyme in solution, N_{\pm} : rightward and leftward electrons, g : guanine radicals

D_{\pm} : 1D diffusivities, f : flip rate, v : e^- speed, Ω reservoir volume, L : DNA length, m : oxidation rate, k_{on} : deposition rate, k_{off} : desorption rate of reduced enzymes on DNA.

Model reduction

Drop derivatives in equation for R_a ; obtain “outer” solution in x and t :

$$R_a \approx \frac{1}{m + k_{\text{off}}} \left(v(N_+ + N_-)Q + k_{\text{on}} \left(\frac{\Omega}{L} \right) R_b \right)$$

Reduced, non-dimensional equations are:

$$\begin{aligned} \frac{\partial Q}{\partial t} &= -U(1 - \sigma)(N_+ + N_-)Q + \nu \frac{\partial^2 Q}{\partial x^2} + \sigma R_b, \\ \frac{dR_b}{dt} &= U(1 - \sigma) \int_0^1 (N_+ + N_-)Q dx - \sigma R_b, \\ \frac{\partial N_+}{\partial t} + U \frac{\partial N_+}{\partial x} &= \left[F + \frac{\sigma}{2} UQ \right] N_- - \left[F + \left(1 - \frac{\sigma}{2} \right) UQ \right] N_+ - gUN_+ + \frac{\sigma R_b}{2}, \\ \frac{\partial N_-}{\partial t} - U \frac{\partial N_-}{\partial x} &= - \left[F + \left(1 - \frac{\sigma}{2} \right) UQ \right] N_- + \left[F + \frac{\sigma}{2} UQ \right] N_+ - gUN_- + \frac{\sigma R_b}{2}, \\ \frac{\partial g}{\partial t} &= -U(N_+ + N_-)g, \end{aligned}$$

$\sigma = \frac{m}{m + k_{\text{off}}}$: effective binding rate per enzyme (competition between electron release m and desorption k_{off})

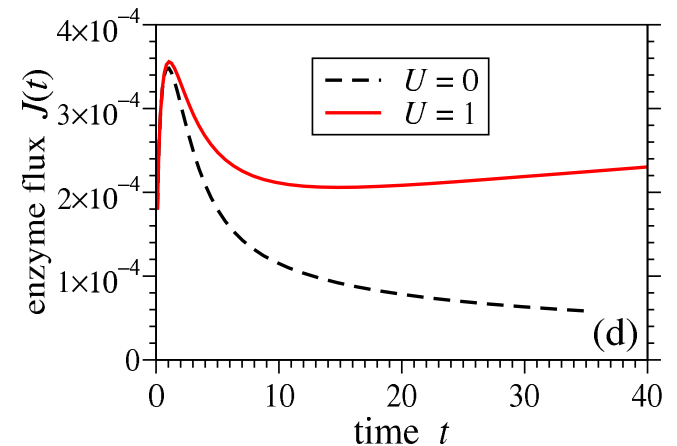
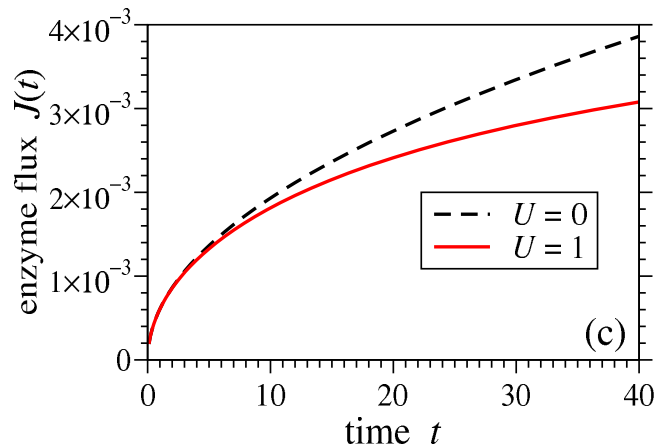
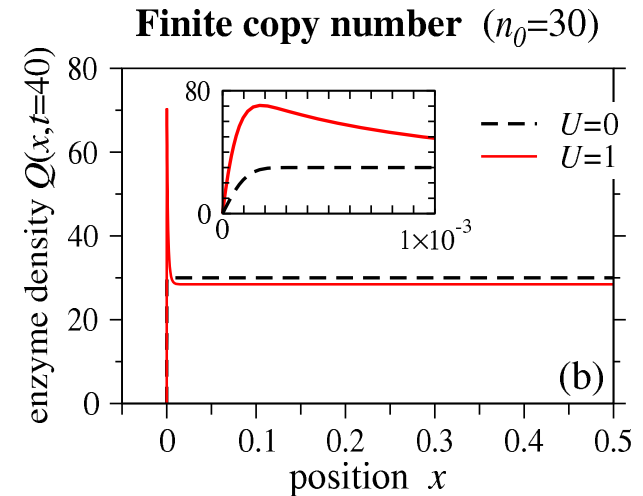
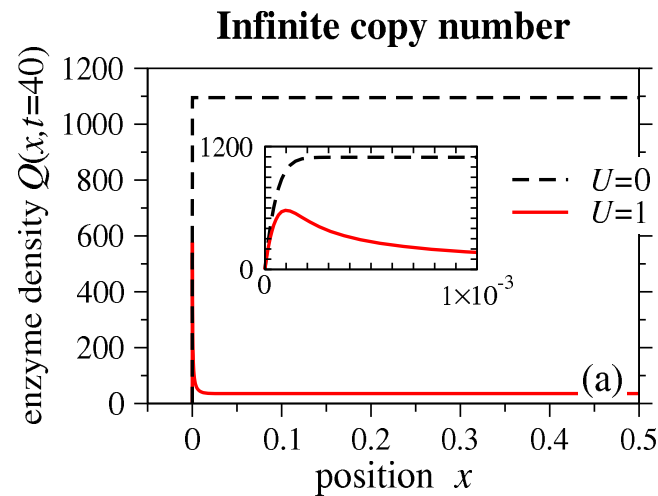
Reduced model

- Dimensionless diffusivity, electron speed, flip rate: $\nu = \frac{D_+}{k_{\text{on}}L^2}$, $U = \frac{v}{k_{\text{on}}L}$, $F = \frac{f}{k_{\text{on}}}$
- Modified flip rates due to enzyme re-attachment: $F \rightarrow F + \frac{1}{2}UQ$ when $\sigma = 1$.
- Numerical scheme: Finite differences on non-uniform grid. Typical $\nu \sim 10^{-10}$, $F \sim 10^5$, $\sigma \sim 1 \Rightarrow$ cluster mesh points near boundary, use stiff solver in time.
- Reservoir dynamics: $R_b(0) \equiv n_0$: copy number of MutY (≈ 30 in *E. coli*). Infinite copy number limit: $R_b(t) = n_0 \quad \forall t$.
- $U = 0$: passive enzyme limit (no CT)
- Estimate time τ_s for enzyme to reach lesion by

$$\int_0^{\tau_s} J(t) dt = 1$$

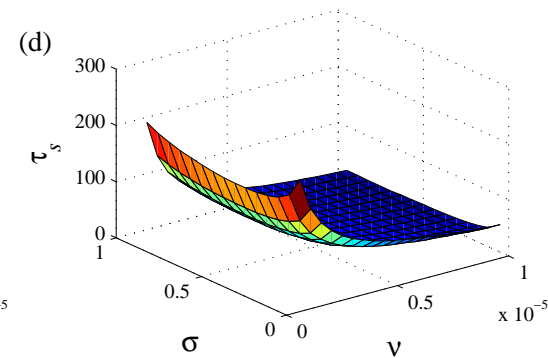
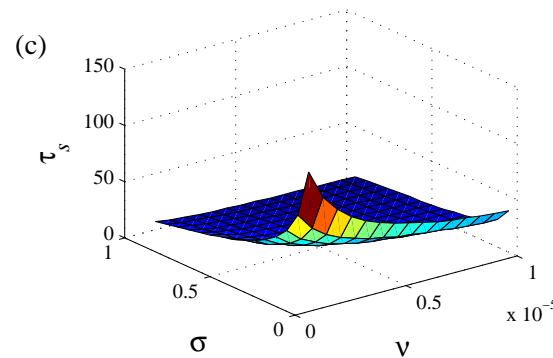
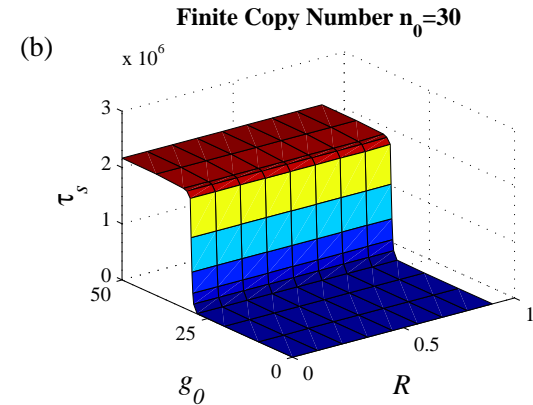
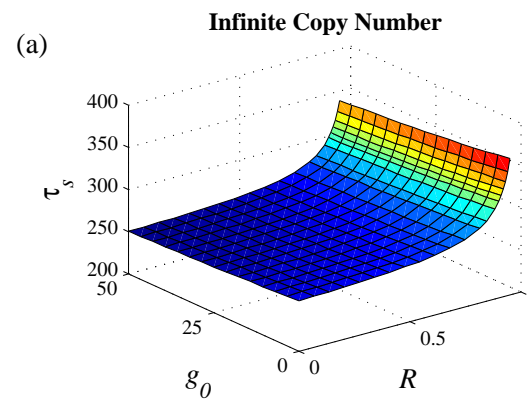
where $J(t) = 2\nu \left. \frac{\partial Q}{\partial x} \right|_{x=0}$.

Enzyme Profiles/Fluxes



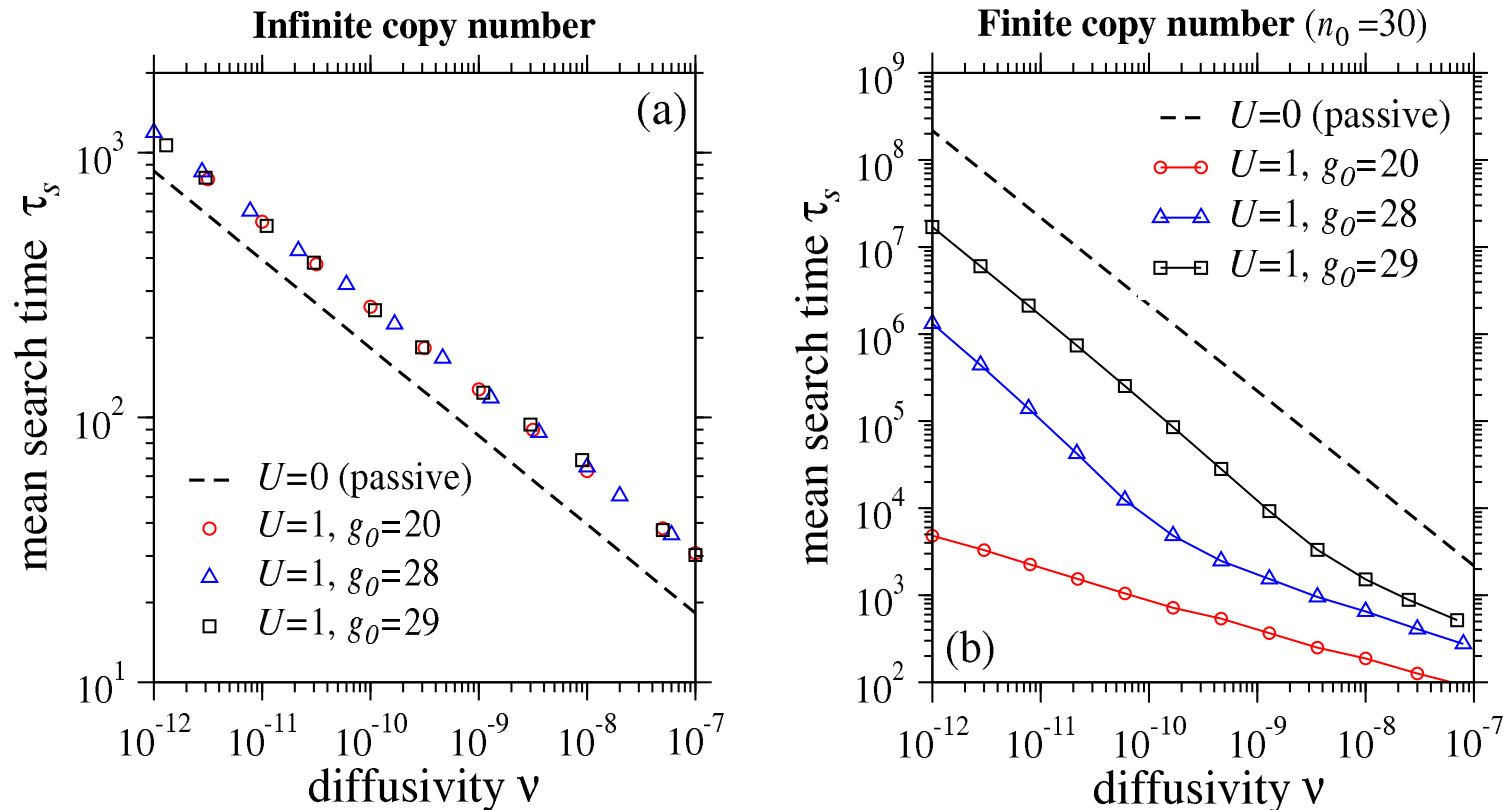
Enzymes colocalize near lesions due to spatially dependent desorption $\propto (N_+ + N_-)Q$.

Search Times



τ_s : search time, g_0 : initial OxoG number, R : lesion's electron reflectivity, σ : enzyme binding affinity, ν : enzyme diffusivity along DNA.

Search Time Dependence on ν

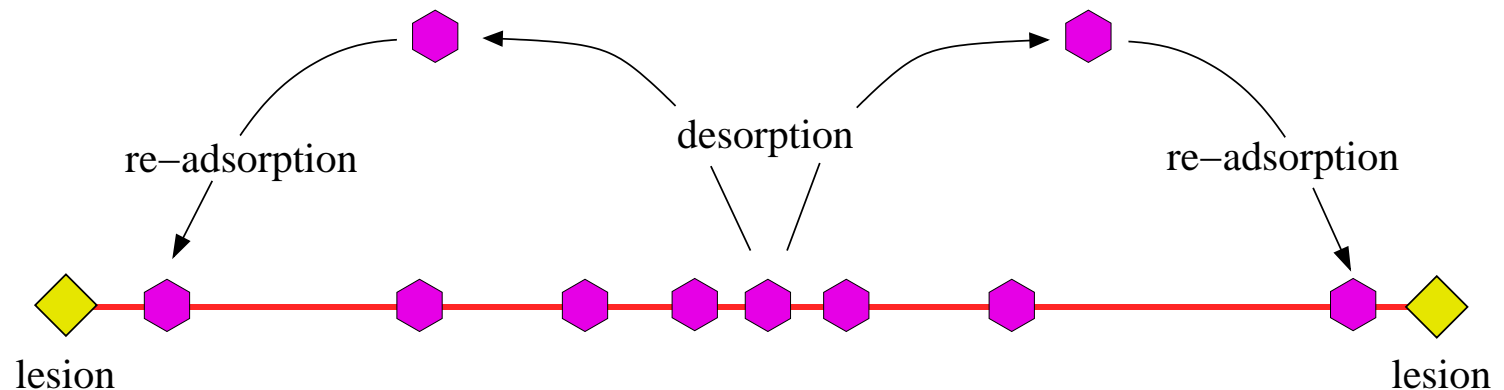


For wide range of diffusivities ν , (a) Infinite CN: $\tau_s = O(\nu^{-1})$ insensitive to g_0 . (b) Finite CN: τ_s extremely sensitive to g_0 . Scaling switches from $O(\nu^{-1}) \rightarrow O(\nu^{-1/3})$

CT accelerates search only in finite CN case.

Conclusions

- Studied discrete and PDE models of Charge Transport (CT) mediated enzyme kinetics.
- Discrete broadwell model improves over facilitated diffusion
 - Statistics of enzyme binding for lesion-free DNA
 - Density profiles/scaling results from MC simulations for DNA with lesions
- PDE model improves over discrete model. Included diffusion along DNA, redox-dependent binding kinetics and “reservoir” effects.
 - Can yield search time on order of seconds
 - CT acceleration due to spatially dependent desorption and enzyme “recycling”





Extensions

- Comparison of discrete and PDE models
- Effect of small copy number \Leftrightarrow chemical master equation
- PDE asymptotics for $F \gg 1$, $\sigma \sim 1$, $\nu \ll 1$
- Other enzyme binding mechanisms with spatially dependent desorption



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